Original Article

Short-range bioaerosol deposition and recovery of viable viruses and bacteria on surfaces from a cough and implications for respiratory disease transmission

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ABSTRACT

Knowledge of respiratory bacterium/virus distribution on surfaces is critical for studying disease transmission via the contact route. Here, we investigated the bioaerosol deposition and distribution on a surface from a cough experimentally. A cough generator was used to release bacterium/virus-laden droplets. A solid surface was placed in front of the cough generator at different relative distances ($D=0.2$, 0.5, 0.8, and 1.1 m) and angles ($\theta=30^\circ, 60^\circ$, and 90°). Benign bacteria and bacteriophages were used separately. Results showed that droplet jet directly impinged upon the surface and then spread out along the surface. The distributions of droplet volume and viable microorganisms along the surface were unimodal. We then identified the impaction region based on the droplet flow field from a particle imaging velocimetry technique, which corresponded with the peak position and high-volume area. The impaction region contained around 83% of droplet volume along the vertical axis of the surface. The peak position, peak value, and width of the impaction region were related to D and θ . The micro-organisms inside the droplets did not affect the droplet distribution on near surfaces. The front surface can work as a partition to block the cough jet and protect people behind, and can be smaller when it is installed closer to the coughing person. This work demonstrates a methodology to obtain distribution and viability of microorganism deposited on surface, and suggest guidelines to setting up a protective partition as a possible intervention method against disease transmission.

1. Introduction

Every year, communicable respiratory diseases cause absence from work, lost worker productivity (Fisk, 2000), 3-5 million severe illness cases and even 290,000 to 650,000 deaths by influenza (WHO, 2018). There are four different exposure pathways in the communicable respiratory disease transmission process: (Atkinson and Wein 2008; Jones and Adida 2011; Lei et al. 2018; Nicas and Jones 2009) (1) direct/indirect contact transmission, (2) large droplet spray transmission, (3) inhalation of inspirable droplets, and (4) inhalation of respirable airborne transmission. Pathway (1) involves direct contact which indicates bodyto-body contact with an infected person, or indirect contact, also denoted as fomites, in which a susceptible person contacts contaminated intermediate surfaces. Pathway (2) means large droplets directly spray onto facial membranes from a cough or sneeze. Pathway (3) corresponds with droplets of 10-100 μ m in aerodynamic diameter, which deposit onto the upper respiratory tract. Pathway (4) is for the particles smaller than 10 μ m in aerodynamic diameter, which deposit onto the upper/lower respiratory tract and

pulmonary region. The relative contribution of each pathway depends on the types of pathogens (Lei et al. 2018), surrounding environment and infection sites in the airways (Jones and Adida 2011). Studies show that airborne transmission (i.e. pathway 3) is one important pathway for influenza and severe acute respiratory syndrome viruses (SARS) to spread (Cowling et al. 2013; Tellier 2006; Tellier 2009; Yu et al. 2004). However, the contact transmission is still an important route for the respiratory diseases (Lowen et al. 2008; Nicas and Jones 2009; Jones and Adida 2011).

Indirect contact disease transmission involves the following steps: deposition and survival of bacteria/viruses from respiratory activities; bacterium/virus transfer to hands and to facial membrane by contact; and infection. Field studies reveal that the viable influenza virus appears on surfaces in offices, households, day care centres (Boone and Gerba 2005; Boone and Gerba 2010), and hospitals (Otter, Yezli, and French 2011; Weinstein and Hota 2004). Researchers also found that human-occupied rooms contain much more bioaerosols than non-occupied rooms (Bhangar, Huffman, and Nazaroff 2014; Bhangar et al. 2016; Qian et al. 2012). Human respiratory activity (e.g. coughing or sneezing) is one of the important sources to contaminate these indoor surfaces. When we cough, the large droplets (initial diameter larger than 60 μ m) can be transmitted in the air jet for as far as 1.5 m – 2 m away horizontally before being deposited onto the ground (Liu et al. 2017; Xie et al. 2007). The smaller droplets initially travel as a cloud, lose momentum, and mix with and follow the background airflow. The cloud of small droplets could span approximately 7-8 m far away from the infector under the initial releasing velocity of up to 10-30 m/s (Bahl et al. 2020; Bourouiba 2020). They may deposit on environmental surfaces by turbulence (Tang et al. 2006; Xie et al. 2007). The pathogen on a surface can migrate broadly through hand touching to other surfaces (Lei et al. 2017) or through resuspension via human walking (Qian and Ferro 2008). Among these surface contamination processes, we can imagine that the near surfaces facing the coughing source will contain much more bacteria/viruses, which should be more likely to cause infection and contaminate more surfaces when touched by hands. Therefore, knowing the bacterium/virus concentration and distribution on a surface near the cough source is important and valuable for infection risk assessment and control.

There is limited research focusing on the deposition and distribution of bioaerosol onto near surfaces from a cough. Chao, Wan, and Sze-To (2008) studied the expiratory droplet transportation and deposition in a hospital ward. Their study showed that gravitational settling was more important for the deposition of larger expiratory droplets. For the airborne droplets, the deposition velocity onto the side wall was comparable to that onto the upward-facing surfaces. Sze To et al. (2009) experimentally studied the expiratory aerosol dispersion and deposition in aircraft cabins, showing that 35% of the droplets in weight were deposited on the seat in front and 4% of the droplets were deposited on the side seat. Wong et al. (2010) studied the bioaerosol nuclei deposition on the plates placed at floor level in a test chamber. They showed that the background flow had an influence on distribution. There were more viable bacteria at the floor section near the wall opposite to the injection point than other areas. Kunkel et al. (2017) studied the size-resolved dynamics of coughing bioaerosol transportation and deposition within three rooms in one apartment (0.5 m, 3 m, and 5 m away). They showed that the largest *Escherichia coli* (*E. coli*) weight happened at 0.5 m and decreased as the distance increased, while the largest phage (virus) weight appeared at 3 m and the smallest weight was at 0.5 m on horizontal settling plates near the floor.

However, these studies focused on airborne aerosol deposition at rather long-range situations with relatively low aerosol velocity (Lai and Nazaroff 2000; Zhao and Wu 2007). In these situations, the microorganisms inside the airborne aerosol can affect the aerodynamics and deposition on floor surfaces (Wong et al. 2010; Kunkel et al. 2017). For a short-range direct deposition onto a surface from a cough with relatively high velocity, it is still unknown whether the bacteria or viruses inside the aerosol would affect the deposition or not. Furthermore, when the high-speed jet of droplet-air mixture directly collides with the surface, the air spreading along the surface will affect the movement of droplets. The droplet jet becomes wider and moves downward due to gravitational force when traveling further. The relative distance and relative angle between the cough and front surface change the jet flow structure near the surface (O'Donovan and Murray 2008) and may affect the bioaerosol flow dynamics, deposition, and distribution along the surface. If the

surface near the coughing person is used as a partition for protective purpose, this information will be essential in designing such a partition.

In this work, the objectives are to investigate the direct deposition of bioaerosols released from a cough, to obtain the viable bacterium/virus distributions on the surface, and to reveal the coughing droplet flow-field near the surface. We used a custom-built generator to simulate a cough and studied the droplet deposition onto a front surface with different relative distances and relative angles. The size-resolved droplet number concentration and viable bacterium/virus distribution on the surface were measured. Two microorganisms were used separately to represent the common bacteria and viruses: *E. coli* (ATCC 11303) and bacteriophage T3 (ATCC 11303-B3).

2. Materials and methods

2.1. Cough generator and artificial saliva solution

The cough generator was a custom-built aerosolization system, which had been used in previous studies (Chao, Wan, and Sze-To 2008; Leung et al. 2013; Sze To et al. 2009; Wan et al. 2007). The released droplet size distribution and initial velocity were tuned based on a real cough (Chao et al. 2009). The size distribution and releasing velocity were measured by an interferometric Mie imaging (IMI) technique and a particle imaging velocimetry (PIV) technique, respectively, and the results are shown in Fig. 1. The measurement setup is shown in Figure 1S in Supplementary Information. The released droplets from the generator had a similar size distribution to a real cough with peak size at $10-20 \mu m$. The droplet velocity was around 12 m/s, similar to the average coughing velocity of 11.7 m/s (Chao et al. 2009). In the experiment, the coughing process lasted 1 s and was repeated 3 times with a time interval of 5 s, controlled by an Arduino system, to simulate a series of frequent coughs. Each cough released 0.075 mL artificial saliva solution.

The artificial saliva solution consisted of 76 g of glycerol and 12 g of Sodium Chloride (NaCl) in 1 litre of sterilized water (Chao, Wan, and Sze-To 2008; Sze To et al. 2009). The non-volatile material accounted for 6% in volume of the initial droplet volume, similar to the actual volume ratio of human respiratory fluid (Effros et al. 2002).

2.2. Experimental setup and solid surface for deposition

Experiments were conducted in a room with controlled temperature and relative humidity at $22^{\circ}C \pm 1^{\circ}C$ and $72\% \pm 4\%$, respectively. The droplets, a mixture of artificial saliva solution and microorganisms, were released from the cough generator positioned in the mouth of a thermal manikin. A solid surface was placed in front of the thermal manikin as shown in Fig. 2a. The background air velocity near the experimental setup was around 0-0.1 m/s, measured by a flow meter (7575-X, Q-track, TSI, USA).

The solid surface for deposition was a smooth polyvinyl chloride (PVC) plate of 0.5 m \times 0.5 m \times 0.6 mm (length, width, and thickness). The surface was clean and there was no *E. coli* or bacteriophage on the surface before the experiment. The surface was marked by horizontal and vertical lines to indicate the sampling positions of 4×4 cm² grids, as shown in Fig. 2b. The origin of the grids was at the position pointed by the cough generator. The positive x-axis was in the right direction and the positive y-axis was in the upward direction.

Figure 2

2.3. Experimental procedure and studied cases

In this work, real bacteria *E. coli* and virus bacteriophage (phage for short) were employed. We first prepared a 200 mL *E. coli* or phage solution with concentration of 10⁷ colony forming unit (CFU)/mL or plaque forming unit (PFU)/mL. Then, we load the mixture of artificial saliva solution and the microorganisms into the cough generator for aerosolization. The air jet together with aerosolized droplets directly collided with and spread along the PVC plate surface. After droplet deposition, the PVC plate was cut into small pieces with size of 4×4 cm² according to the pre-marked grid with sterilized scissors. Each small piece was further cut into two symmetrical pieces. One part was used to count the size-resolved bioaerosol by a microscope (Ni-E, Nikon, Japan). The other part was put into a tube with 5 mL sterilized water to extract the deposited *E. coli* or phage in water. Then, the pour plate method and top agar layer method were used to measure the viable *E. coli* and phage concentrations in water respectively and were described in detail in Section 2.4. The deposited viable *E. coli* and phage numbers on surface could then be calculated.

The collection process of bacteriophage or *E. coli* after deposition on the surface was completed at around 40 minutes after aerosolization and deposition. After deposition on the surface, the microdroplets might still undergo evaporation which is the key process to inactivate bacterium/virus (Xie et al. 2006). Microscope observation was conducted, and it was found that the evaporation was completed within the collection time. The final equilibrium status of droplets was related to the environmental temperature and relative humidity which were well-controlled during the experiment. Thus, the measured CFU/PFU here can be regarded as the initial bacterium/virus concentration on the surface from a cough, compared with a few days' or months' lifetime of the microorganism on a surface.

In this experiment, the relative distance $D=20, 50, 80,$ and 110 cm and relative angle $\theta=30^{\circ}, 60^{\circ}, 90^{\circ}$ were studied. Two microorganisms, *E. coli* and bacteriophage were used, respectively. So, in total, 24 cases were studied, and each case was repeated 3-4 times.

2.4. Bacterium and virus solution preparation and cultivation method

E. coli and bacteriophage used in this work were supplied from the American Type Culture Collection (ATCC). *E. coli* is the Gram-negative rod-shaped bacterium with typical size of 0.5-2 µm, and the phage is a double-stranded DNA coliphage and the characteristic size is about 60-200 nm. They are commonly used as the surrogates of bacterium and virus respectively in experimental studies (Kunkel et al. 2017; Lai et al. 2018; Yoon et al. 2007).

For the *E. coli* experiment, the *E. coli* was cultured in advance in Tryptone soya broth (TSB) solution for 24 h in an incubator at a temperature of 37 ºC. Then the *E. coli* solution was centrifuged at 4,000 RPM for 15 minutes to obtain *E. coli* pellets. The *E. coli* pellets were then resuspended in 200 mL artificial saliva solution. The *E. coli* concentration of the final solution for cough generator was 10⁷ CFU/mL.Serial dilution was conducted to dilute the *E. coli* solution. Then, pour plate method was used to measure the *E. coli* concentration in a solution. Firstly, target *E. coli* solution of 1 mL was transferred into a petri dish by a pipette. Then, melted sterilized Tryptone soya agar (TSA) solution of around 25 mL with temperature of around $52 \degree C$ was poured into the same petri dish. The solution was mixed by gentle shaking in the petri dish and the solution was then solidified by cooling to room temperature. Then the petri dish was inverted, sealed by the parafilm, and put in an incubator at a temperature of 37 ºC for around 24 hours. Then, the colony forming units (CFUs) on the petri dish were counted. The *E. coli* concentration in initial solution could be calculated by the CFU number on plate and the corresponding dilution ratio.

For the bacteriophage experiment, the high titre bacteriophage solution (up to 10^{10-11} PFU/mL) was prepared in advance. In the experiment, the solution of around 100 µL was diluted into 200 mL artificial saliva solution with a final concentration of 10⁷ PFU/mL. First, serial dilution was conducted to dilute the target phage solution and obtain the diluted solutions with different dilution ratios. Then, top agar layer method was used to measure viable phage concentration for each of the diluted solutions: preparing solidified agar plates in advance, mixing 0.2 mL target phage solution with 0.2 mL *E. coli* host solution in a tube, waiting for 15 minutes, then mixing quickly with 3 mL 52ºC soft agar [in g/L: nutrient broth, 25; agar power, 7], and pouring onto the prepared agar plate. The plates were inverted after solidification and put into an incubator for 10 hours. Then the plaque forming units (PFUs) were counted and the viable phage concentration was calculated by the PFU number and corresponding dilution ratio.

For the preparation of high titre phage solution, the bacteriophage T3 was first cultured in its *E. coli* host solution for 10 h in an incubator at 37 °C. The top agar layer method was then used to prepare the plates with bacteriophage plaques. The top layer of the plates with more than 100 PFUs were scraped off into a flask, stirred for 60 minutes at 37 ºC, and then centrifuged at 10,000 g for 15 min. The supernatant was centrifuged again at 28,000 g for 30 min. The bacteriophage pellet left at the bottom was then suspended into the buffer solution and the high titre phage T3 solution was then stored in a refrigerator at 4 ºC. The detailed protocol can be found in reference (Kunkel et al. 2017). But in the last step, the phage pellet was resuspended into the Tris buffer $\left[\text{in } g/L \right]$: Tris, 6.05, PH 7.4; NaCl, 5.8; MgSO₄·7H₂O, 2] instead of the albumin-dextrose-saline (ADS) solution to avoid changing the wetting property of the solution.

The influenza A virus concentration in nasal washes from a small panel of subjects has been shown to range from 6×10^2 TCID₅₀ to 2×10^7 TCID₅₀ (the full name: 50% Tissue Culture Infective Dose) (Murphy et al. 1973). TCID₅₀ is the virus dose that successfully infects 50% of the tissue culture assays. So here we prepared solution with unfavourable concentration (i.e. upper limit of the concentration range) between 10⁷ – 10⁸ CFU/mL or PFU/mL as the *E. coli* and bacteriophage concentration.

2.5. Particle Imaging Velocimetry (PIV) setup

The Particle Imaging Velocimetry (PIV) technique was employed to measure the released droplet velocity from the generator and to characterize the droplet velocity field near the solid surface before colliding with the surface. In the PIV experimental setup, a laser sheet was used to light up the droplets, and a camera was positioned perpendicular to the laser sheet to capture the droplet positions. Then, droplet velocity and direction can be calculated by the time interval and position difference between two sequential moments. The time interval of double exposure was 30-80 μ s, depending on the measured velocity magnitude. The PIV setup for measuring droplet velocity near the surface is shown in Figure 2S in the Supplementary Information. Each measurement covered an area of 7 cm \times 5 cm (length \times height). Measurement was conducted at 4-6 positions for each case to acquire the whole picture of velocity field near the surface.

2.6. Measurement of size-resolved droplet by microscope and droplet volume calculation

The PVC sample for the microscope measurement was $2 \text{ cm} \times 4 \text{ cm}$ in size. Uniform sampling method was used to take 36 pictures of droplets on the surface by the array of 4×9. It was ensured that the result was independent of the sampling number by comparing results of sampling 24 (4×6) and 54 (6×9) points.

The droplet volume, *V*, was calculated by the following spherical cap equation (Fu et al. 2018; Leung et al. 2013; Tadmor 2004; Wang et al. 2020) due to the rather small bond number at the static status ($Bo = \rho gh^2$) $\gamma_L = 10^{-4}$, *h*: droplet height, γ_L : liquid surface tension), which indicates that surface tension dominates in microdroplets.

$$
V = \frac{\pi (1 - \cos \theta)(\sin^2 \theta + 1 - \cos \theta)}{\sin^3 \theta} D^3
$$
 (1)

where θ is the apparent contact angle, and D is the contact diameter of a droplet on the surface. The contact angle of the droplet was measured by a goniometer (Biolin Theta Contact Angle Meter C204A, Biolin Scientific, Sweden). The *E. coli*-laden droplet contact angle was measured as 41º, and the bacteriophageladen droplet contact angle was 56º.

2.7. E. coli/bacteriophage survivability calculation

The following equation was used to calculate *E. coli*/bacteriophage survivability in the whole processes of coughing, deposition, and evaporation:

$$
S = \frac{N}{c \cdot (V/r)}\tag{2}
$$

where *N* (CFU/cm² or PFU/cm²) is the viable *E. coli*/bacteriophage number per unit area on the surface by cultivation, *c* (CFU/mL or PFU/mL) is the viable *E. coli*/bacteriophage concentration of the solution before aerosolization, and V (mL/cm²) is the total volume of the droplets per unit area on the surface at equilibrium status. The equivalent droplet volume before evaporation was determined by *V*/*r*, where *r* is the ratio of droplet volume at equilibrium status to the initial volume, and *r* was measured to be 13.34% by a goniometer (Biolin Theta Contact Angle Meter C204A, Biolin Scientific, Sweden).

3. Results

3.1. Size-resolved droplet number concentration and distribution on surface

Figure 3

When the cough jet impinged on the flat surface, the air jet spread along the surface. Both large and small droplets deposited on the surface close to the impaction point due to inertia impaction, while some smaller droplets changed direction, spread with the air jet, and deposited on the surface far away from the impaction point. This process was visualized and further discussed by the droplet velocity field from the PIV results in Section 3.5. Fig. 3 shows the images of deposited bacteriophage-laden droplets for the case of *D*=50 cm, θ =90° from the position *y*=0 cm (origin) to the downward edge at *y* = -23.5 cm. It shows that both droplet size and number on the surface decreased gradually from the origin to the edge of the surface. At the origin, both large and small droplets were densely distributed on the surface, while at the edge, the small droplets were sparsely distributed.

Figure 4

Fig. 4 shows the size-resolved number concentrations of the bacteriophage-laden droplets along the y-axis on the surface under different cases. Four droplet sizes with contact diameters of $3-20 \mu m$, $20-50 \mu m$, $50-$ 100 μm and 100-500 μm were presented. When *D*=20 cm, the overall number concentrations of droplets along the surface demonstrated the bimodal distributions. When *D*=50, 80, and 110 cm, the droplet number distributions were the unimodal distributions, but they were asymmetric and upward skewed. For *D*=50 cm and θ =90°, the number distribution of droplets was an approximately symmetric distribution. As θ decreased from 90[°] to 30[°] or *D* increased from 50 to 110 cm, the distribution leaned downward more heavily, and the peak position also moved downward. The peak positions of droplet number concentrations of different sub-size ranges were almost the same, except for the cases of *D*=20 cm. It indicated in most cases, droplets of different sizes travelled all together without separation in the vertical direction.

When *D* increased from 20 to 110 cm, the peak value of the overall number concentration decreased from around 2×10^4 to 3×10^3 #/cm², and most of the deposited droplets were smaller than 50 μ m in diameter. This is due to the fact that the cough jet became wider in radial direction and the droplet number concentration in the cough jet decreased when traveling forward. It is also found that some droplets larger than $100 \mu m$ in diameter appeared on the surface in the case of $D=20$ cm. The formation of these large droplets is suspected to be the consequence of droplet agglomeration, because for a smaller *D*, there was a higher chance for the droplets to deposit on the same position and agglomerate on the surface.

Under the same distance *D,* the peak number concentrations along the surface for the three different angles were found to be in the same magnitude. It is because under the same distance, the number concentrations of the droplets in the cough jet were similar, and the impaction velocities were in the same magnitude for different surface angles, as shown in Section 3.5 later. Therefore, the effect of the surface angle on the peak number concentration is moderate, compared with the effect of the relative distance *D*. The possibility of agglomeration was also similar for different angles under the same distance, resulting in the similar peak number concentration of large droplets.

3.2. Phage-laden droplet volume distribution on surface

Figure 5

Fig. 5 shows the distribution of phage-laden droplet volume concentration $(\mu m^3/cm^2)$ on the surface. The droplet volume concentration was the overall volume of droplets with different sizes per unit area at the sampling position. The volume of each droplet was calculated by Eq. (1) according to the contact diameter on the microscope images. For all cases, the droplet volume concentrations demonstrated the unimodal distributions. It was found that the distributions fit the following skew normal equation (3), and the best-fit parameters are listed in Table 1S in the Supplementary Information.

$$
f(x) = k \times \frac{2}{\omega} \times \varphi\left(\frac{x - \epsilon}{\omega}\right) \times \varphi\left(\alpha\left(\frac{x - \epsilon}{\omega}\right)\right) \tag{3}
$$

where
$$
\varphi(x) = \frac{1}{\sqrt{2\pi}} e^{-\frac{x^2}{2}}
$$
, $\phi(x) = \int_{-\infty}^{x} \varphi(t) dt = \frac{1}{2} \left[1 + erf\left(\frac{x}{\sqrt{2}}\right) \right]$

In Fig. 5, it was observed that with an increase of distance or decrease of relative angle, the position of the peak shifted gradually downward (in negative y-axis direction). The skewness of the distribution decreased from around 0.9 to nearly zero when the angle increased from 30º to 90º. When the distance increased or the angle decreased, the variance of the distribution increased, meaning that the droplet volume was more sparsely distributed on the surface.

3.3. Plaque forming unit (PFU) distributions on the surface and virus survivability

Figure 6

Fig. 6 shows the viable bacteriophage number concentration distribution along y-axis. The PFU distribution was also fitted by Eq. (3) and the parameters are listed in Table 2S in the Supplementary Information. It was seen that the viable bacteriophage distribution was similar to the droplet volume distribution on the surface, as shown in Fig. 5. The detailed comparison is shown in Figure 3S in Supplementary Information. It indicates that the number of viable virus contained in the droplets is proportional to the droplet volume. It should be noted that the size of a virus (\sim 0.06 μ m) was much smaller than that of the droplets (\sim 10 μ m), so the droplet dynamics were not affected by the virus inside. The virus survivability in the cough and deposition process was calculated and shown in Table 1. It ranged from 12.9% to 23.6% with the overall mean value of 17.7% \pm 5.7%. There was no clear relationship between the survivability and the relative distance or angle. This indicates that, for the short-range deposition, the survivability is independent of the relative distance and angle of the surface. Therefore, the viable microorganism concentrations on the near

surface mainly depend on the droplet dynamics and deposition process. It should be noted that the values of the survivability depend on the aerosolization process, cultivation time, targeted microorganism, environmental conditions, etc. and are very different in different practical scenarios. Therefore, the values of the survivability obtained in this study cannot be directly used in risk assessment. More specific studies are essential to investigate the microorganism survivability in different situations.

Table 1

Figure 7

The viable bacteriophage concentrations along the x-axis (Figure 7) demonstrated the symmetric unimodal distributions, which were different from the upward skewed unimodal distribution in the y-axis direction. The distributions were well fitted with the normal Gaussian equation, which was a special case of skewed normal Eq. (3) with $\alpha =0$ and $\epsilon=0$, and the parameters are shown in Table 3S in the Supplementary Information. The variance increased as the relative distance *D* increased, and it was larger with smaller relative angle θ . It shows that the viable virus distributions spread wider along the horizontal direction of the surface as the *D* increased or θ decreased, which was similar with that along the vertical direction of the surface. The peak position was the same as the mean position at $x = 0$ for all *D* and θ , but the peak value, decreased greatly as *D* increased.

Figure 8

The peak positions of the viable bacteriophage concentration were not always located at the origin but changed with the relative distance and angle. Fig. 8a shows the peak positions of the viable bacteriophage concentration on the y-axis and Fig. 8b shows the corresponding peak values against the relative distance and angle. The peak position moved downward gradually as the distance *D* increased due to the gravitational force. For each distance *D*, the peak position was lower for a smaller relative angle. The peak positions matched with a parabolic equation, indicating the effect of gravitational force in the vertical direction. Fig. 8b shows the values of the viable bacteriophage concentration at peak positions under different cases. They decreased sharply when the relative distance increased and were fitted by an exponential equation. The fitting parameters in Fig. 8a & 8b are reported in Tables 4S and 5S in Supplementary Information.

3.4. Droplet velocity field near the surface by particle image velocimetry (PIV) technique

Figure 9

Fig. 9 shows the velocity field of cough droplets near the surfaces for the cases of *D*=50 cm. The velocity fields of the other studied cases are presented in Figure 4S in the Supplementary Information. In the PIV measurement, the cough droplets were the seed particles, Therefore, Fig. 9 represents the velocity field of the cough droplets. According to the PIV result, as *D* increased from 20 to 110 cm, the droplet jet spread wider in the radial direction from 5 cm, to larger than 35 cm during the flight. The droplet jet velocity decayed from 11 m/s at the nozzle of the cough generator to around 5, 1.8, 1.1, and 0.75 m/s at the position close to the surface (around 5 cm apart), when *D* was equal to 20, 50, 80, and 110 cm respectively.

It was observed that the droplet jet first travelled toward the surface with a specific flow direction and after impaction it became a parallel spreading flow along the surface. When $\theta = 30^\circ$, the spreading flow was mainly in the upward direction (positive y-direction). As θ increased to 90 $^{\circ}$, the spreading flow became symmetrical, spreading both upward and downward along the surface after impaction. By observing the direction of the droplet jet at the near wall region (within 1 cm above the surface), two regions were identified: the impaction region and the spreading region where the flow was parallel to the surface, illustrated by the red bracket and red arrow in Fig. 9, respectively. The range of the impaction region and the ratio of droplet volume in the impaction region to the overall volume along the y-axis is summarized in Table 2. The length of the impaction region gradually increased with the increase of *D* and was insignificantly affected by θ . The droplet volume in the impaction region accounted for 83.0% \pm 3.6% of the overall volume along the y-axis. By comparing the impaction region with droplet number/volume distributions in Figures 4 and 5, it was found that the impaction region corresponded with the high number/volume area. It indicates that, in the impaction process, both the large and small droplets directly deposited in the impaction region. Large droplets were deposited by inertial impaction, and small droplets were brought close to the surface and deposited by turbulent diffusion. Some of the small droplets spread along the surface, following the spreading air, and were finally deposited by turbulent diffusion.

Table 2

3.5. Distribution of E. coli droplet and comparison with that of bacteriophage droplet

Bacterium *E. coli* was also used to study the deposition and distribution of bacteria-laden droplets onto the near surfaces. The studied cases were the same as that of the virus deposition and the results are shown in the Supplementary Information. The number concentration and distribution of *E. coli* droplets were similar to that of the bacteriophage droplets. The colony forming unit (CFU) distribution also matched well with the droplet volume distribution under a suitable scaling. The mean survivability of *E. coli* for studied cases was 24.1% \pm 10.3%. The volume distributions of *E. coli* droplets and bacteriophage droplets were compared. Both the distributions and the peak positions along the surface were similar, meaning that the microorganisms inside the droplets did not affect the droplet deposition on near surfaces. This was different from some of the research works in the literature (Wong et al. 2010; Kunkel et al. 2017), which showed that the bacteria or viruses inside the droplets can affect the deposition because of the irregular shapes of the airborne nuclei. In this work, for short-range situations, the evaporation process was not completed before deposition, so most of the airborne droplets were larger than 10 μ m in diameter. They were much larger than the bacterium or virus inside and were in spherical shape as if there were no microorganism inside. So, the droplets containing microorganisms have the same aerodynamic forces as that without microorganisms, resulting in a similar deposition pattern on near surfaces.

4. Discussion

Surface cleaning is an effective way to cut the contact route and help end the epidemic transmission of nosocomial pathogens although the debate continues about this causal relationship (C. Cohen, B. Cohen,

and Shang 2015; Otter, Yezli, and French 2011; Tschudin-Sutter et al., 2017). In the contact precaution, the cleaning and disinfection of the area near the patient should be conducted frequently (Jane et al., 2007; Lisa et al., 2018; Lynne and Raymond, 2003). Our research reveals that the impaction region with the length of around 21 cm contains around 83.0% of viable deposited bacteria/viruses along the surface. Thus, the cleaning and disinfection of the high concentration areas immediately after a cough could effectively reduce infection risk and minimize the further spreading of bacteria/viruses through contact. On the other hand, our findings also indicate that the viable virus/bacterium can be brought by the spreading air and deposited far away from the impaction point. Therefore, the cleaning process should be taken with caution.

The distributions of the deposited bacteria/viruses on the surfaces obtained in this work could improve the accuracy of estimating contact exposure. In modelling of infection risk of the contact route (Jones and Adida, 2011; Sze‐To et al., 2014; Lei et al., 2018; Nicas and Jones, 2009), the viable bacterium/virus distribution on the surfaces near the infector is conventionally assumed to be uniform and the surface is considered as a whole unit for bacterium/virus transfer. The current finding of the bacterium/virus distribution could be integrated into the model, working as the initial microorganism concentration of different touching positions. It should be noted that the number of viable bacteria/viruses on the surface depends on the viabilities of the targeted microorganisms. Our measured microorganism concentration on the surface cannot represent all microorganisms, but the relative spatial distribution of the concentration would be helpful in assessing the relative risk, and here we also demonstrate a methodology for future analysis.

The results in this work suggest some guidelines in setting up a partition as a possible intervention method to prevent the direct droplet spray on nearby people. When there is a vertical partition in front of a sick person who coughs, the cough jet together with the virus will spray on the partition surface, while protecting the people behind the partition. The size of the partition should be large enough to, at least, cover the spray area. According to the results of the droplet flow field, the spray area is centred at the level of mouth with a diameter related to the distance between the person and the partition. Therefore, for a farther distance, such as 110 cm from the sick person, a higher partition is needed because the aerosol spreads wider during the flight. When the distances are 20 cm, 50 cm, 80 cm and 110 cm, the height of the partition should be at least 10 cm, 15 cm, 20 cm, and >30 cm higher than the level of the person's mouth respectively. Since the spray area is symmetric about the person's mouth, the required widths of the partition are at least 20 cm, 30 cm, 40 cm, and >60 cm respectively with the person's mouth at the middle. When a smaller partition with suitable size is installed at a position closer to the sick person, it is not necessary to install another partition with larger size further away because most of the aerosols are blocked by the front partition. It should be noted that the suggestions above are based on the horizontal coughing posture result (i.e. $\theta = 90^\circ$). Head posture with different angles are not considered.

5. Conclusions

In this work, we study the bioaerosol deposition and distribution onto a flat surface from a cough. It is found that when the cough jet impinges on the surface, both the large and small droplets directly deposit on the surface, forming a high concentration area, and then only some small droplets flow with the spreading air. The distribution of viable *E. coli*/phage fits well with skew normal distribution. The impaction region with the length of around 21 cm contains up to 83% of viable deposited bacterium/virus on the vertical line along the surface. The peak position and the peak value of the virus distribution are correlated with the relative distance and angle. The impaction velocity varies from 5 m/s to less than 1 m/s under different relative distances, while the survivability is similar for different distances. This indicates that the impaction velocity does not affect the microorganism survivability. The *E. coli*-laden droplet has similar distribution with that of a phage-laden droplet, meaning that the micro-organisms inside the droplets do not affect the droplet deposition onto near surfaces. The near surface could work as a protective partition to block cough spraying. The size of the partition is determined by the flow field of the cough jet near the surface; closer to the coughing person, a smaller partition is required. The mechanism of the deposition and distribution of cough droplets can help set up surface cleaning and disinfection strategies and provide guidelines for partition sizes in front of the infector.

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Declarations of interest

None.

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Figure 1. Droplet size distribution and releasing velocity from the cough generator, where f is number frequency of droplet, dp is droplet size, and the unit of the velocity in the legend is m/s.

Figure 2. (a) Schematic diagram of the experimental setup, (b) the solid surface with sampling points

Figure 3. Images of bacteriophage-laden droplet of the case of $D=50$ cm, $\theta=90^\circ$ at different positions along vertical line (a) $y = 0$ cm, (b) -8 cm, (c) -16 cm, (d) -23.5 cm

Figure 4. Size-resolved droplet number concentration along the vertical line (y-axis) on the surface. The number concentration of each sub-size range is stacked. The mean value and standard deviation (error bar) of each sub-size are obtained from the experiment repeated three times.

Figure 5. Distribution of phage-laden droplet volume concentration on surface at distances of $D = 20, 50$, 80, 110 cm. The mean value of volume and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

Figure 6. Viable bacteriophage number concentration distribution in the vertical line (y-axis) along the surface. The mean value of PFU and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

Figure 7. Viable bacteriophage concentration distribution in the horizontal line (x-axis) along the surface. The mean value of PFU and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

Figure 8. (a) The peak position of the viable bacteriophage concentration on the vertical line and (b) the corresponding peak values under different cases.

Figure 9. Droplet velocity field near surface for the cases of relative distance *D* = 50 cm. The unit of the velocity in the legend is m/s.

Table 1. The phage survivability in coughing and deposition processes at four relative distances and three angles of the surface

Cases	$D=20cm$	$D=20cm$	$D=20cm$	$D=50cm$	$D=50cm$	$D=50cm$		
	$\theta = 30^\circ$	$\theta = 60^\circ$	$\theta = 90^\circ$	$\theta = 30^\circ$	$\theta = 60^\circ$	$\theta = 90^\circ$		
Impaction region (cm)	$-8 < y < 3$	$-5 < y < 5$	$-6 < y < 5$	$-16 < y < 3$	$-16 < y < 5$	$-11 < y < 10$		
Volume ratio	79.8%	81.4%	86.7%	81.6%	87.3%	95.0%		
Cases	$D=80cm$	$D=80cm$	$D=80cm$	$D=110cm$	$D=110cm$	$D=110cm$		
	$\theta = 30^\circ$	$\theta = 60^\circ$	$\theta = 90^\circ$	$\theta = 30^\circ$	$\theta = 60^\circ$	$\theta = 90^\circ$		
Impaction region (cm)	$-24 < y < 0$	$-22 < y < 3$	$-20 < y < 5$	$-24 < y < -5$	$-25 < y < 0$	$-20 < y < 3$		
Volume ratio	78.6%	83.0%	89.1%	63.4%	82.3%	88.3%		
Mean value of impaction				Length of impaction region $D=20$, 50, 80, and 110 cm: 11, 21, 25, and 26 cm				
region	with mean value of 21 cm							
	Volume ratio D=20, 50, 80, and 110 cm: 82.6%, 88.0%, 83.6%, and 78.0%							
	with mean value of $83.0\% \pm 3.6\%$							

Table 2. Position ranges of impaction region of different cases

Notes: 'Impaction region (cm)' means the covered area by impaction along the y-axis on the surface. Volume ratio is the ratio of droplet volume in the impaction region to the overall droplet volume along the y-axis on the surface. The length of impaction region and volume ratio at each *D* are the mean values of the cases of three angles under the same *D*.

Supplementary material

Short-range bioaerosol deposition and recovery of viable viruses and bacteria on surfaces from a cough and implications for respiratory disease transmission

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Figure 1S. IMI setup of the measurement of droplet size distribution immediately from the cough

Notes: for IMI, a laser sheet is used to illuminate the transparent droplet. A camera is used to collect the refraction pattern, which is put at the downstream of laser with angle around 80º depending on the distance between laser sheet and camera. Then, the droplet size can be calculated from the refraction pattern based on the particle sizing equation.

Figure 2S. PIV setup of the flow field measurement near the solid surface

Figure 3S. Comparison between PFU from cultivation and droplet volume on *y*-axis

Figure 4S. Droplet velocity field near surface for difference relative distances and angles. The unit of the velocity in the legend is m/s.

Figure 5S. Size-resolved E-coli-laden droplet concentration and distribution on surface

Figure 6S. Comparison between CFU from cultivation and droplet volume on surface

Figure 7S. Comparison between *E-coli* laden droplet volume and phage-laden droplet volume

		20 cm			50 cm			80 cm			110 cm	
	30	60	90	30	60	90	30	60	90	30	60	90
	5.7e7	1.05e8	.28e8	4.42e6	2.7e7	2.9e7	.45e6	2.92e ₆	4.67e6	4.69e5	5.0e5	3.7e5
ϵ	-8.15	-5.23	-3.88	-16.58	-0.89	-0.64	-25.93	-2.63	-9.17	-28.34	-27.71	-18.26
ω	7.14	5.36	4.35	14.18	6.93	5.89	18.88	11.89	8.22	22.71	17.99	12.92
α	5.74	2.12	1.37	3.59	-0.65	-1.13	4.465	-0.83	0.79	6.24	.92	1.09
Mean	-2.54	-1.37	-1.08	-5.68	-3.90	-4.16	-11.20	-8.70	-5.09	-10.45	-14.98	-10.66
Skewness	0.88	0.49	0.26	0.743	-0.05	-0.18	0.83	-0.09	0.08	0.90	0.43	0.17
Variance	19.48	13.74	1.05	82.35	39.00	22.30	139.6	104.6	50.97	195.63	161.6	109.18

Table 1S. The parameters of skew normal equations for droplet volume at four relative distances and three angles of the surface

Table 2S. The parameters of skew normal equations for PFU along y-axis at four relative distances and three angles of the surface

		20 cm			50 cm			80 cm			110 cm	
	30	60	90	30	60	90	30	60	90	30	60	90
	.22e3	1.96e3	5.02e3	57.91	140.09	136.64	12.44	37.85	45.77	4.46	4.22	2.97
ϵ	-4.93	1.41	-0.67		2.02	1.66	-23.96			$\overline{}$	-24.17	-18.39
				14.81				12.36	10.60	23.80		
ω	5.54	3.75	2.66	14.51	9.14	7.74	20.18	11.04	9.77	21.95	19.64	16.16
α	1.40	-1.25	0.01	2.37	-1.65	-1.53	8.17	1.23	1.12	20.59	7.66	2.30
Mean	-1.33	-0.92	-0.65	-4.14	-4.22	-3.52	-7.98	-5.53	-4.78	-6.31	-8.63	-6.57
Skewness	0.27	-0.22	θ	0.55	-0.35	-0.31	0.94	0.21	0.18	0.99	0.93	0.53
Variance	17.72	8.61	7.08	96.75	44.60	33.17	151.81	75.29	61.58	175.8	144.28	121.36

Table 3S. The parameters of skew normal equations for PFU along x-axis at four relative distances and three angles of the surface

		20 cm			50 cm			80 cm			110 cm	
	30	60	90	30	60	90	30	60	90	30	60	90
	2.62e3	2.95e3	4.30e3	169.95	374.53	258.16	36.50	65.60	112.4	15.07	11.26	5.63
	θ	θ	θ	θ		θ		0	θ			θ
ω	3.01	3.01	3.02	6.18	5.27	4.90	10.96	8.16	6.78	14.07	12.72	10.98
α	θ	θ		O		$\left(\right)$	O	0	θ			θ
Mean	θ	θ				θ		-0	θ			θ
Skewness	0	θ		θ		θ		0	θ			
Variance	9.06	9.07	9.13	38.24	27.75	24.01	120.12	66.50	45.97	197.96	161.80	120.56

Table 4S. The parameters of fitting equations for peak position ($y = ax^2 + bx$)

	30°	60°	90°
a	9856	$1.025e+04$	$2.094e+04$
	-0.05569	-0.05059	-0.06987
R-square	0.9982	0.9995	0.9976

Table 5S. The parameters of fitting equations for peak value of PFU ($y = a \cdot e^{b \cdot x}$)

 Table 6S. The *E-coli* survivability in coughing and deposition processes at four relative distances and three angles of the surface

Survivability	30°	60°	90°			
20 cm	$46.7\% \pm 26.2\%$	$36.1\% \pm 16.4\%$	$21.9\% \pm 21.8\%$			
50 cm	$17.9\% \pm 5.3\%$	$13.0\% \pm 2.3\%$	$10.6\% \pm 4.6\%$			
80 cm	$23.1\% \pm 5.1\%$	$19.8\% \pm 5.5\%$	$20.9\% \pm 7.4\%$			
110 cm	$14.3\% \pm 3.4\%$	$33.9\% \pm 8.0\%$	$30.9\% \pm 6.7\%$			
Mean Survivability $24.1\% \pm 10.3\%$;						

Note: for the cases of *D*=20 cm, the survivability in a high concentration area is much larger than that in other areas. Some extremely large droplets (1-2 mm in contact diameter) appear there due to spill of droplets from the cough generator, which were not well captured by the microscope and underestimate the droplet volume. These extremely large droplets did not appear in the study of phage-laden droplet deposition.

Figure 1. Droplet size distribution and releasing velocity from the cough generator, where f is number frequency of droplet, dp is droplet size, and the unit of the velocity in the legend is m/s.

81x41mm (300 x 300 DPI)

Figure 2. (a) Schematic diagram of the experimental setup, (b) the solid surface with sampling points 89x48mm (300 x 300 DPI)

Figure 3. Images of bacteriophage-laden droplet of the case of D=50 cm, θ=90º at different positions along vertical line (a) y = 0 cm, (b) -8 cm, (c) -16 cm, (d) -23.5 cm

77x78mm (300 x 300 DPI)

Figure 4. Size-resolved droplet number concentration along the vertical line (y-axis) on the surface. The number concentration of each sub-size range is stacked. The mean value and standard deviation (error bar) of each sub-size are obtained from the experiment repeated three times.

89x123mm (300 x 300 DPI)

Figure 5. Distribution of phage-laden droplet volume concentration on surface at distances of $D = 20$, 50, 80, 110 cm. The mean value of volume and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

87x93mm (300 x 300 DPI)

Figure 6. Viable bacteriophage number concentration distribution in the vertical line (y-axis) along the surface. The mean value of PFU and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

55x57mm (300 x 300 DPI)

Figure 7. Viable bacteriophage concentration distribution in the horizontal line (x-axis) along the surface. The mean value of PFU and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

53x54mm (300 x 300 DPI)

Figure 8. (a) The peak position of the viable bacteriophage concentration on the vertical line and (b) the corresponding peak values under different cases.

53x27mm (300 x 300 DPI)

Figure 9. Droplet velocity field near surface for the cases of relative distance $D = 50$ cm. The unit of the velocity in the legend is m/s.

53x61mm (300 x 300 DPI)

Figure 1. Droplet size distribution and releasing velocity from the cough generator, where f is number frequency of droplet, dp is droplet size, and the unit of the velocity in the legend is m/s.

81x39mm (300 x 300 DPI)

Figure 2. (a) Schematic diagram of the experimental setup, (b) the solid surface with sampling points 89x48mm (300 x 300 DPI)

Figure 3. Images of bacteriophage-laden droplet of the case of D=50 cm, θ=90º at different positions along vertical line (a) y = 0 cm, (b) -8 cm, (c) -16 cm, (d) -23.5 cm

77x78mm (300 x 300 DPI)

Figure 4. Size-resolved droplet number concentration along the vertical line (y-axis) on the surface. The number concentration of each sub-size range is stacked. The mean value and standard deviation (error bar) of each sub-size are obtained from the experiment repeated three times.

89x123mm (300 x 300 DPI)

Figure 5. Distribution of phage-laden droplet volume concentration on surface at distances of $D = 20$, 50, 80, 110 cm. The mean value of volume and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

87x93mm (300 x 300 DPI)

Figure 6. Viable bacteriophage number concentration distribution in the vertical line (y-axis) along the surface. The mean value of PFU and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

92x95mm (300 x 300 DPI)

Figure 7. Viable bacteriophage concentration distribution in the horizontal line (x-axis) along the surface. The mean value of PFU and standard deviation (error bar) at each position are obtained from the experiment repeated three times.

89x91mm (300 x 300 DPI)

Figure 8. (a) The peak position of the viable bacteriophage concentration on the vertical line and (b) the corresponding peak values under different cases.

89x46mm (300 x 300 DPI)

Figure 9. Droplet velocity field near surface for the cases of relative distance $D = 50$ cm. The unit of the velocity in the legend is m/s.

89x102mm (300 x 300 DPI)